

MRI-NUFFT: Non Cartesian operators and trajectories

2026-05-22 – SFB MR-Dynamo

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Neurospin Lab

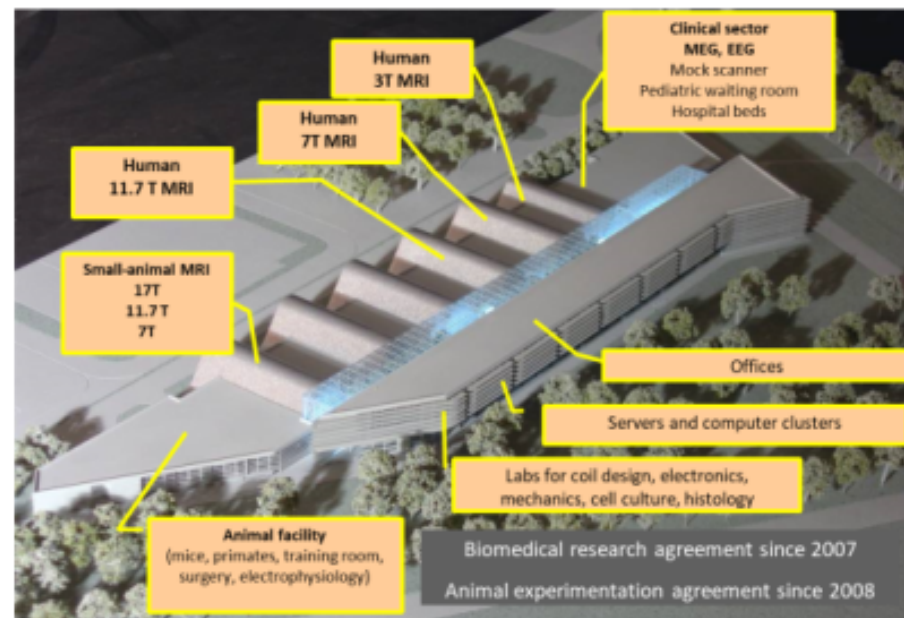
Clinical
MRI



Preclinical
MRI



EEG, MEG



Outline

1. Context
2. Mathematical Operators for Non-Cartesian MRI
3. Trajectories and Gradients
4. The toolbox in practice



1. ■ Context

(Yet Another) Recall on MRI Acquisition

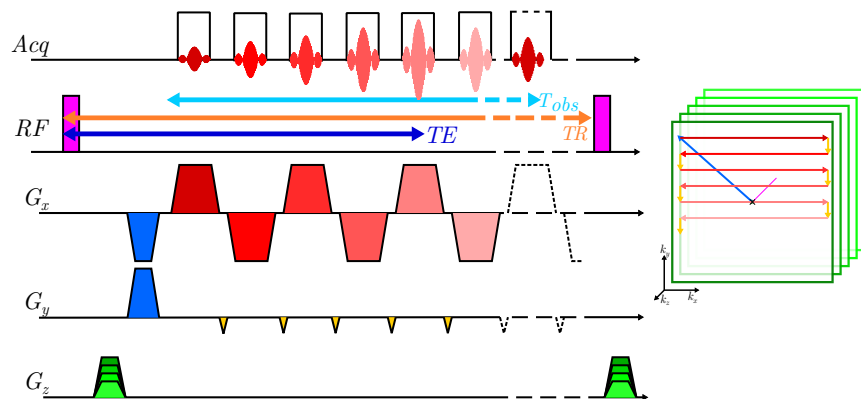


Figure 1: Simple 3D EPI MRI sequence

- MRI is typically acquired using a Cartesian sampling strategy
 - Line-readout EPI, 3D EPI, SMS, ...
 - Undersampling (Acceleration) is limited to sub-sampling along k_x or k_y axis (phase-encoding)

(Yet Another) Recall on MRI Acquisition

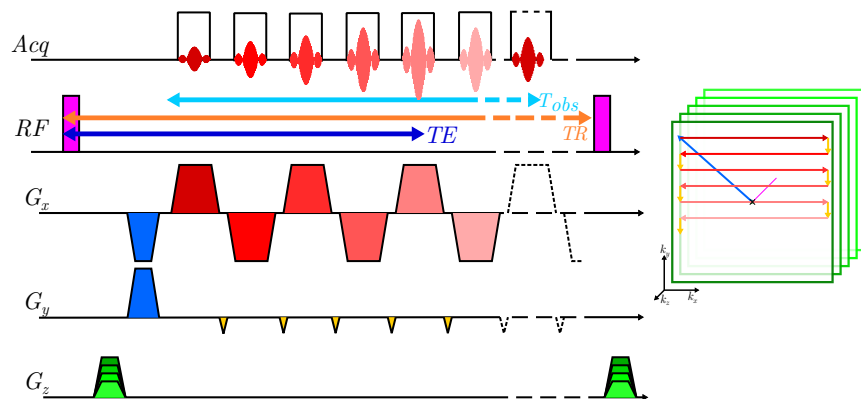
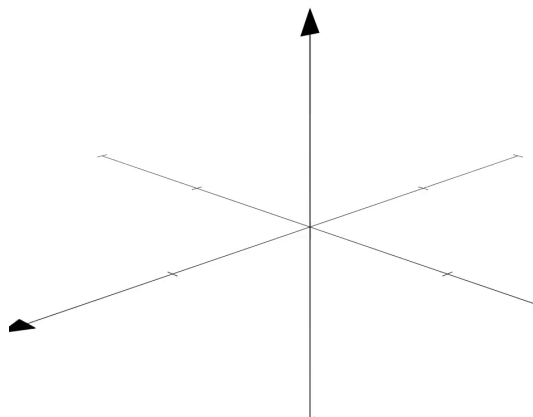
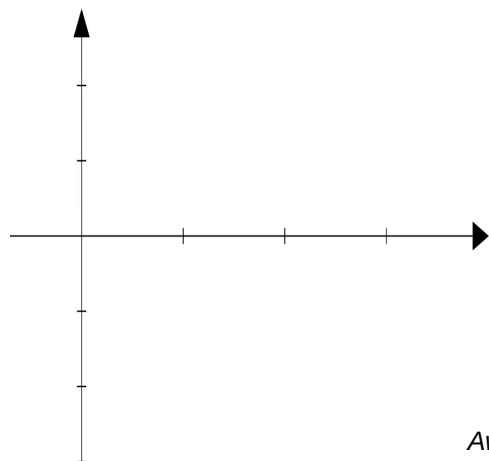


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$$k_u(t) = \frac{\gamma}{2\pi} \int_0^t G_u(\tau) d\tau, \forall u \in \{x, y, z\}$$



Awesome “Manimation”: Courtesy of Chaithya GR

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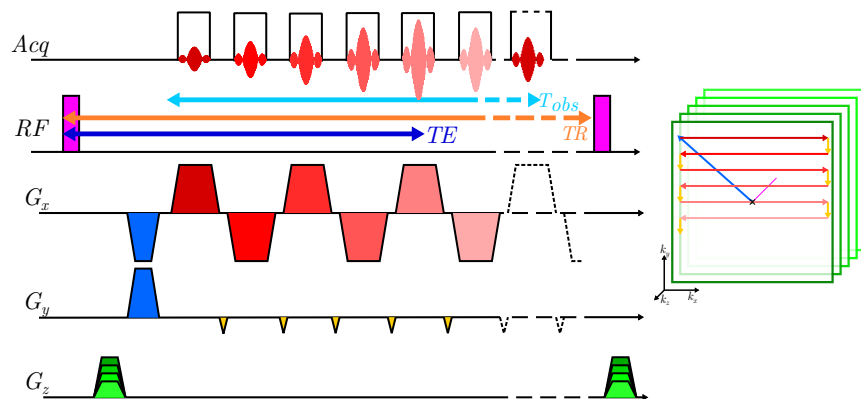


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- There are hardware and safety limits on the gradient

$$\|G_u(t)\|_2 \leq G_{\max}$$

$$\left\| \frac{dG_u(t)}{dt} \right\|_2 \leq \frac{G_{\max}}{\Delta T} = S_{\max}$$

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MRI Reconstruction

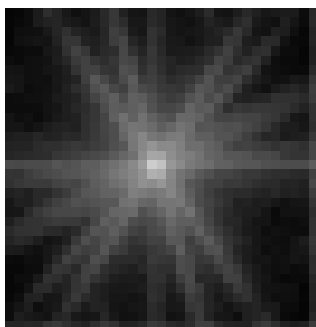
- Solving one (or many) *ill-posed* **inverse problem**

$$y = Ax + \varepsilon$$

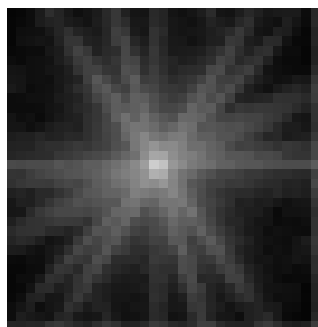
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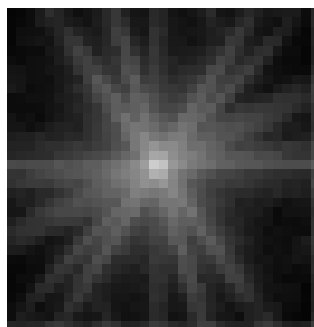
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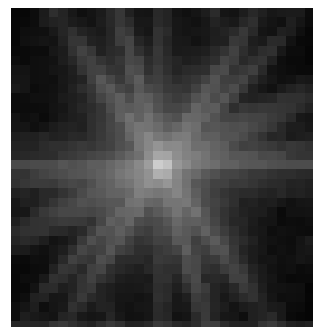
Anatomical MRI



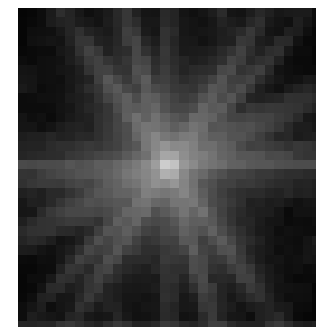
Cardiac /CINE



Quantitative MRI



Diffusion MRI

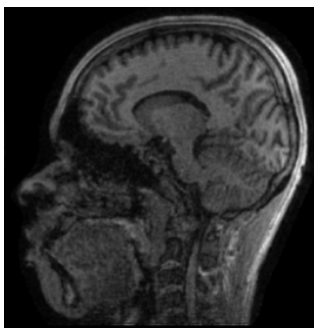


Functional MRI

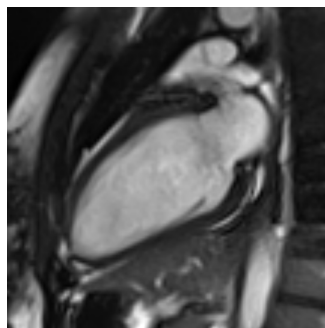
MRI Reconstruction

- Solving one (or many) *ill-posed inverse problem*

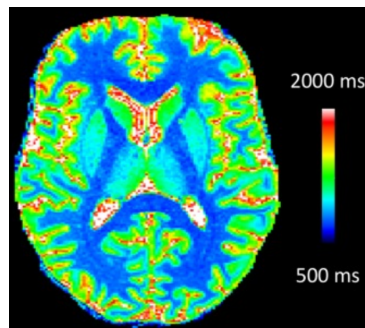
$$y = Ax + \varepsilon \implies x = \mathcal{M}(A, y, \text{priors})$$



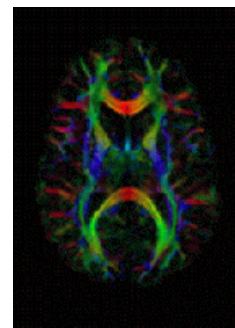
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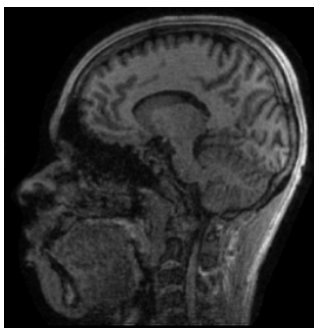


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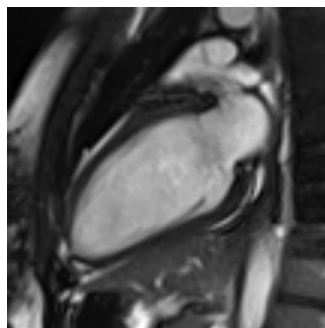
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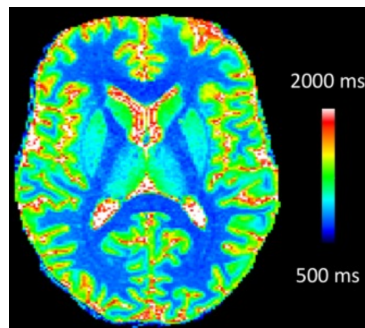
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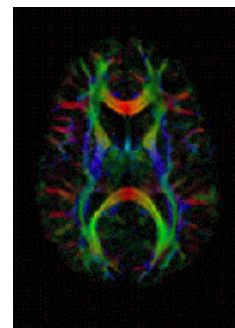
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Functional MRI

Common Goal: Solve the inverse problem

Design (Learn ?) and validate $\mathcal{M}$, A and *priors*

Introducing MRI-NUFFT

- Most MR Toolboxes focus on Cartesian sampling

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- Non-Cartesian: Great potential
 - ✓ Freedom of sampling locations
 - ✓ Increased sampling efficacy
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- But ...
 - ✗ Require expensive Non-Uniform Fourier Transform
 - ✗ Off-Resonance effects
 - ✗ (Re)-design non-Cartesian trajectories for sequences
 - ✗ MR System constraints

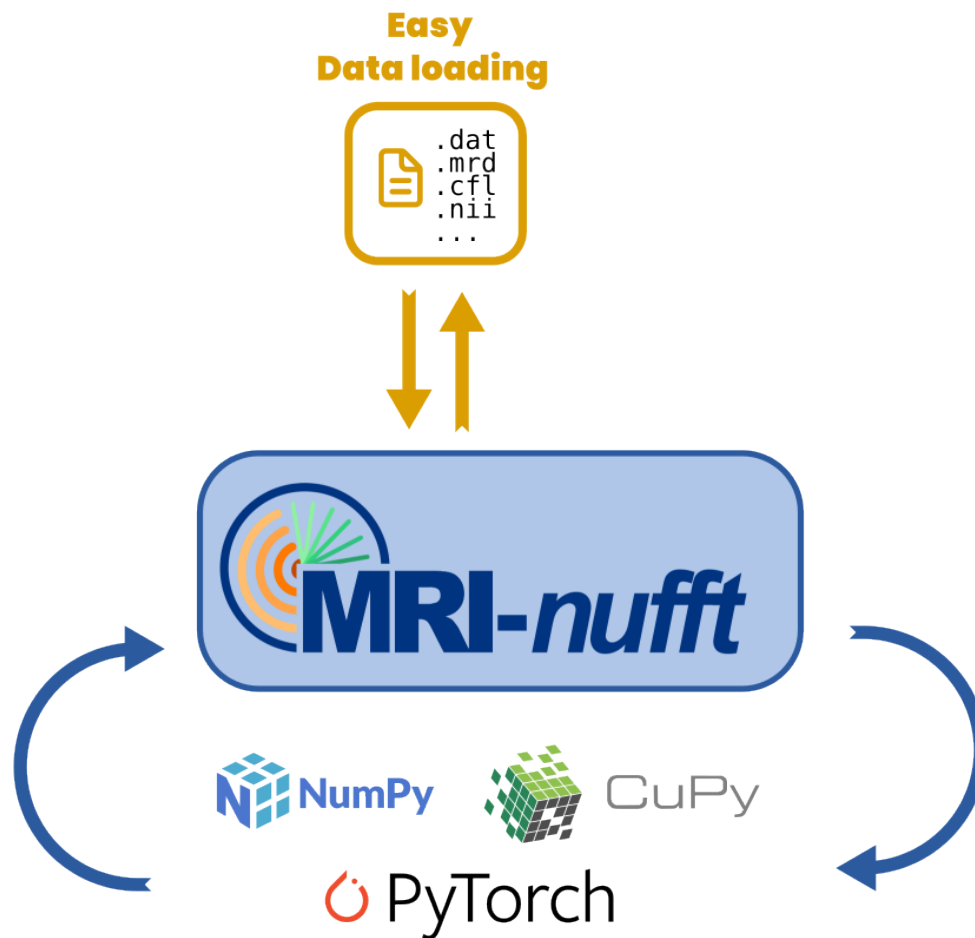
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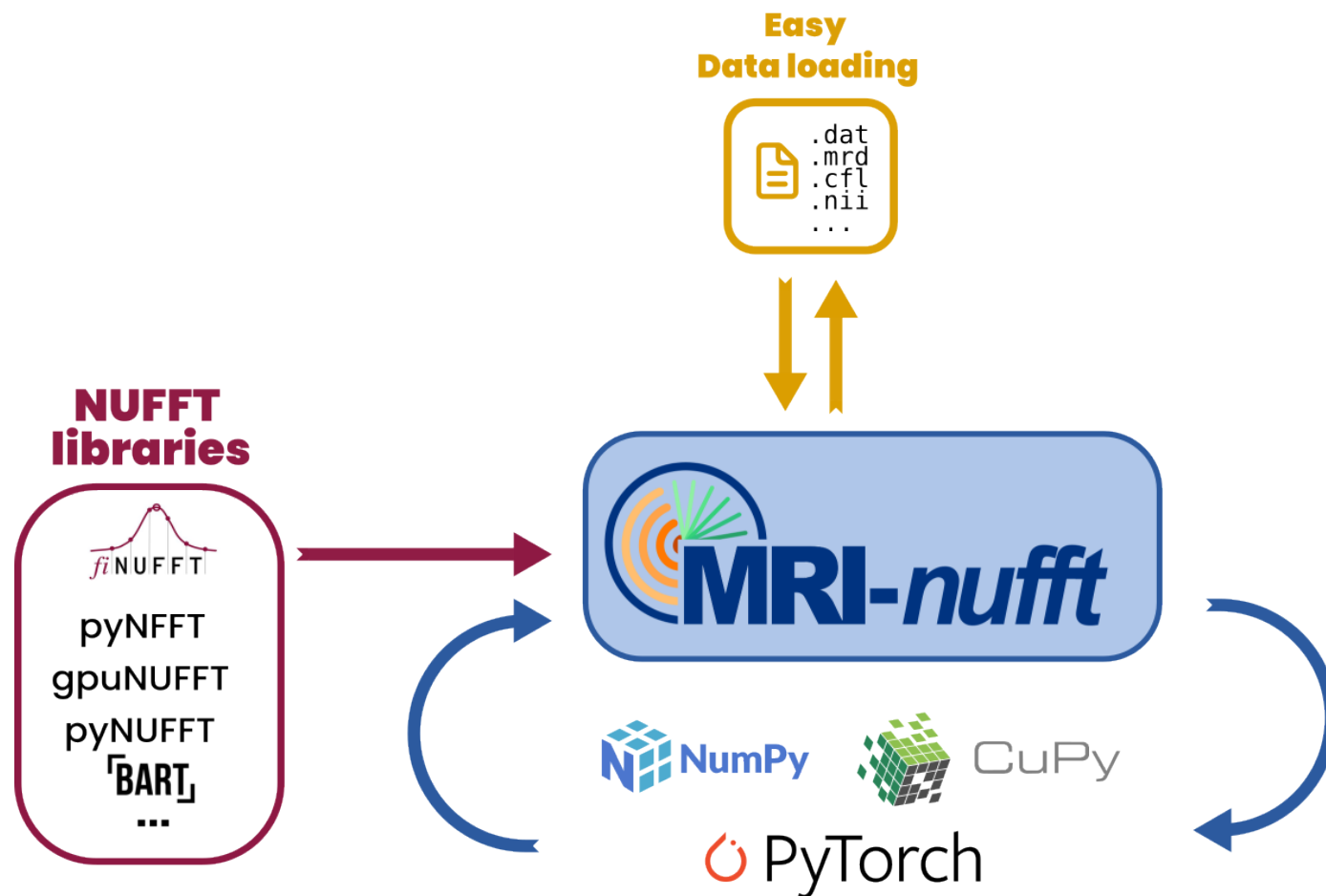
Let's fix this with:



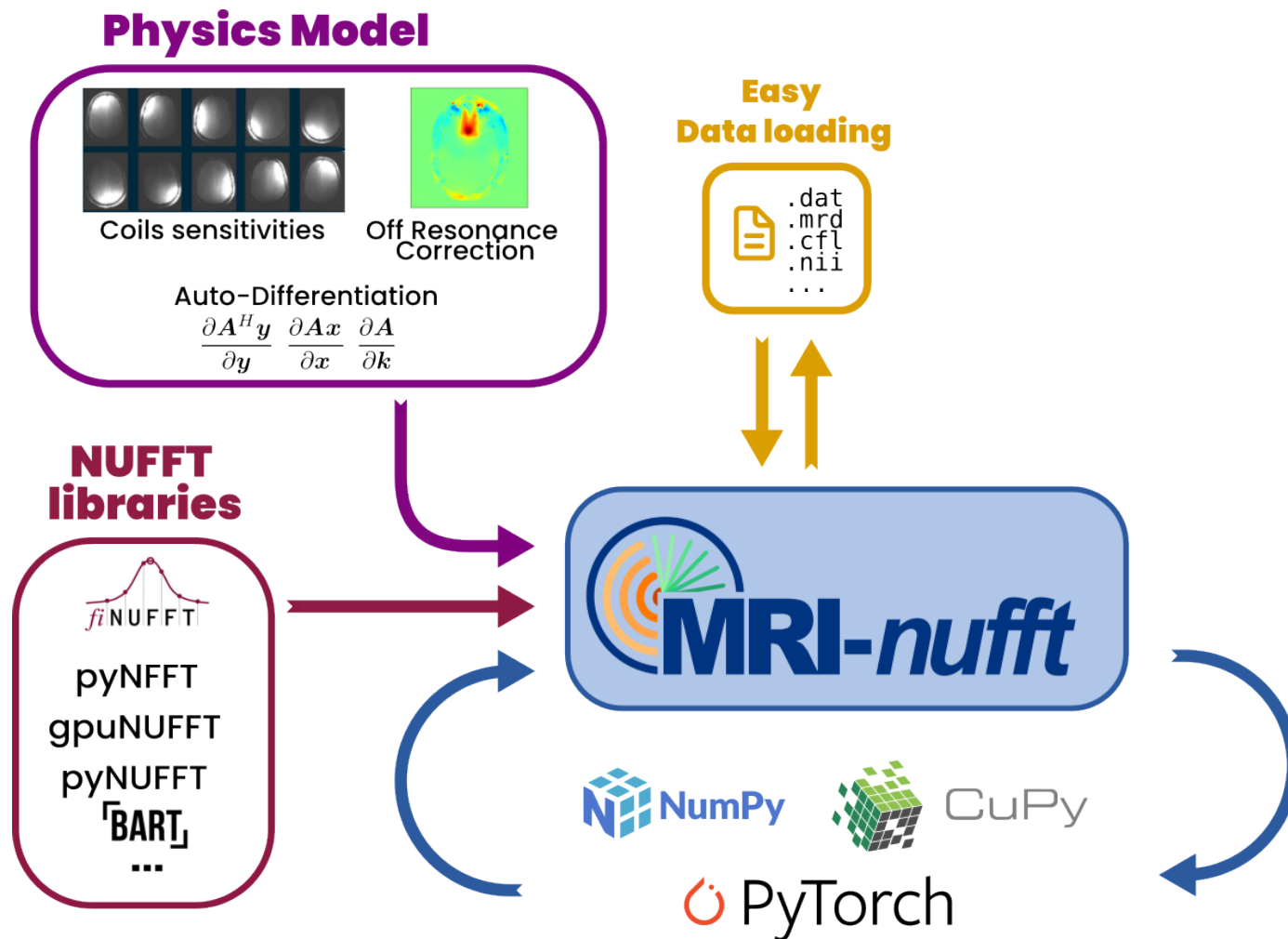
MRI-NUFFT in a Nutshell



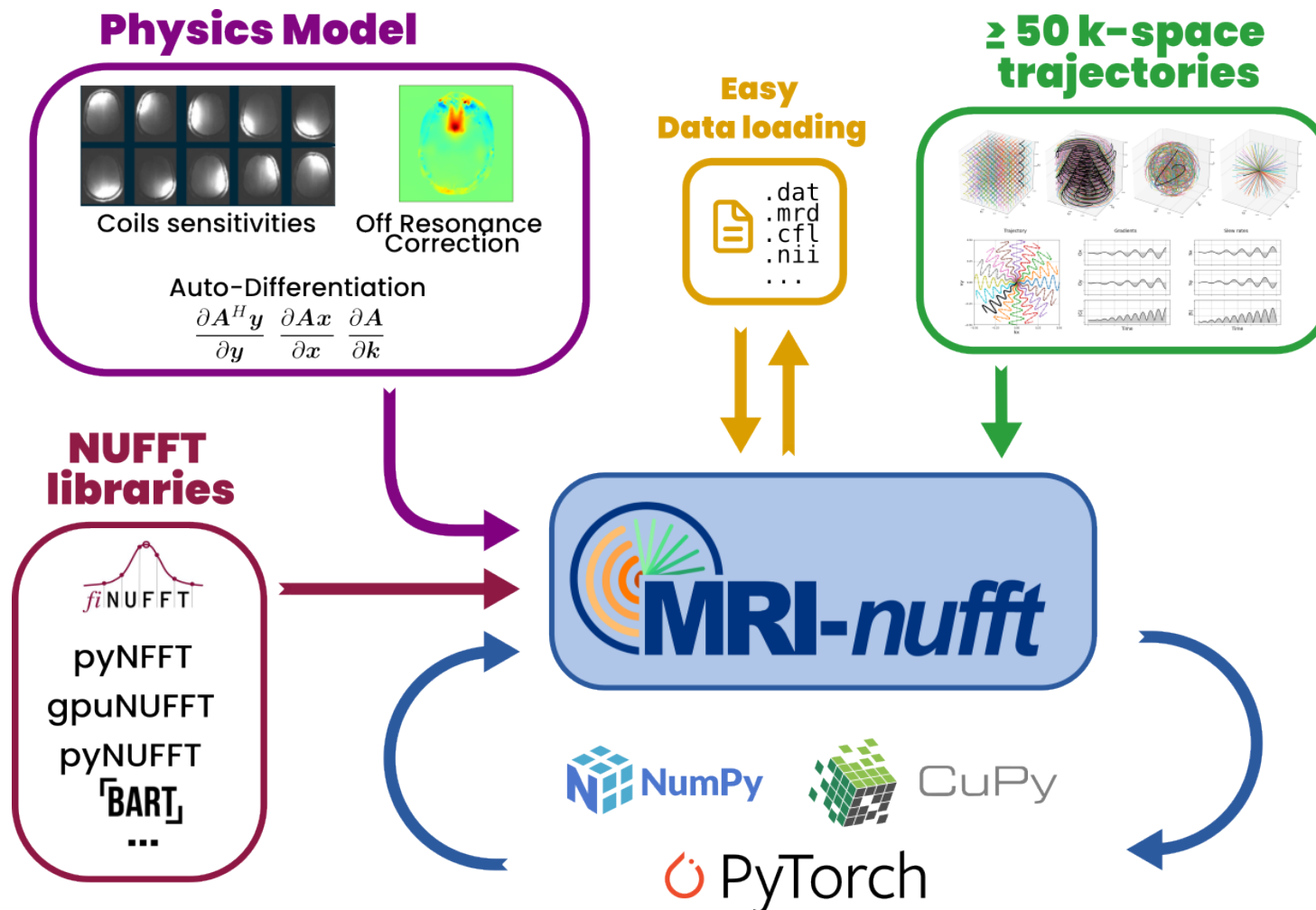
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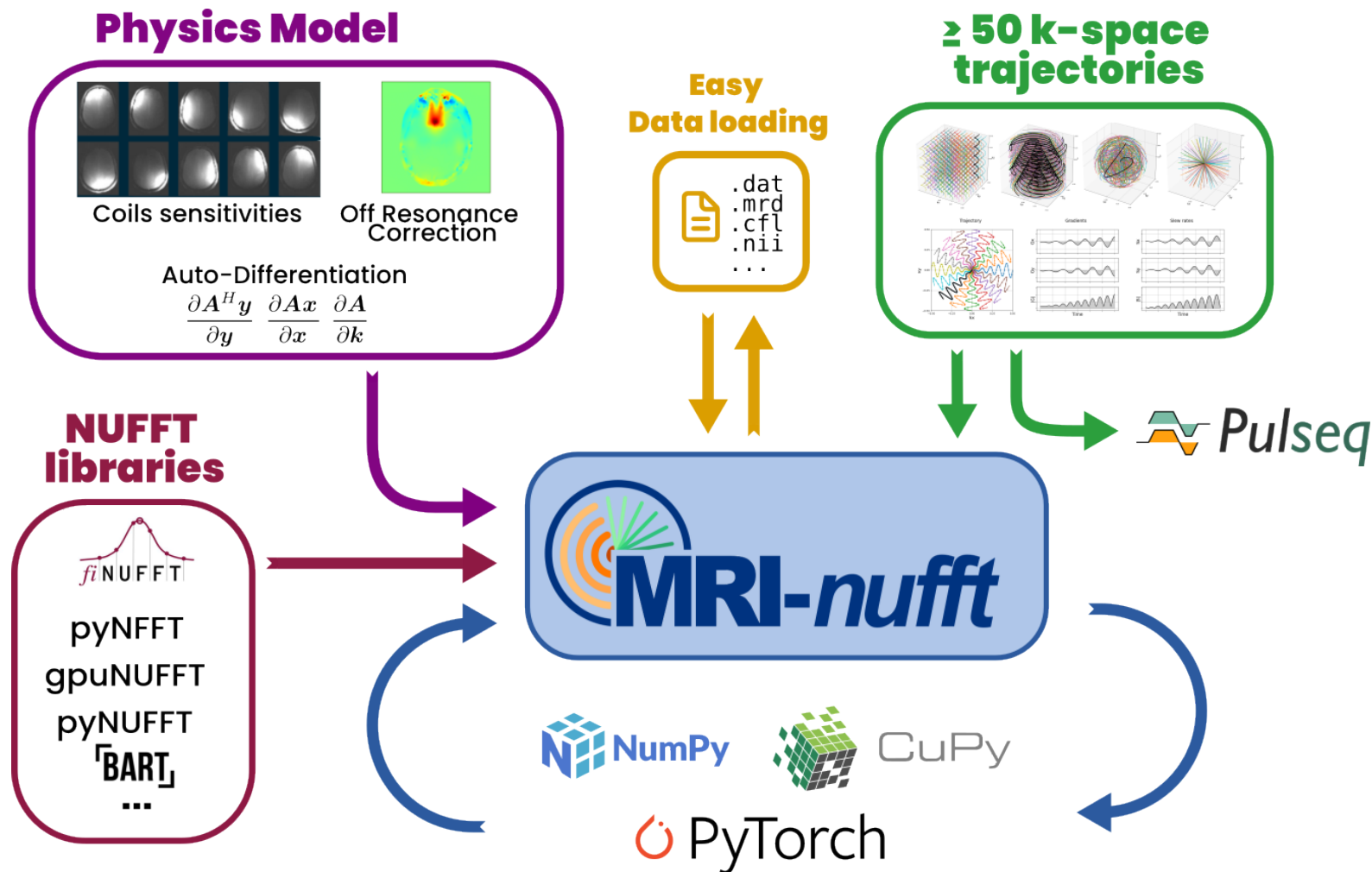
MRI-NUFFT in a Nutshell



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2 ■ Mathematics for non-Cartesian MRI

From FFT to NUFFT

$$y(t) = \int_{\mathbb{R}^d} x(\mathbf{u}) e^{-2\imath\pi \mathbf{k}(t) \cdot \mathbf{u}} d\mathbf{u}$$

$$\forall i = 1 \dots M, j = 1 \dots N \quad y_i = \sum_j x(\mathbf{u}_j) e^{-2\imath\pi \mathbf{k}_i \cdot \mathbf{u}_j}$$

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- In Cartesian settings, *uniform sampling*: $k_i = i \cdot \delta k$, $u_j = j \cdot \delta u$
 - FFT: $\mathcal{O}(N \log N)$

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 - Greedy: Discrete Fourier Transform : $\mathcal{O}(MN)$
 - Smarter: Non-Uniform Fast Fourier Transform $\mathcal{O}(\alpha N \log(N) + M/\log(\varepsilon))$
 1. Interpolation (ε -precise Kernel) to an oversampled grid (α)
 2. FFT
 3. Apodization correction and cropping FOV

Fessler&Sutton, IEEE TSP, 2003.

Barnett et al., 2019

Shih et al., 2021

Non-Cartesian MRI reconstruction



- Inverse problem formulation for MRI

$$\hat{\boldsymbol{x}} = \arg \min_{\boldsymbol{x} \in \mathbb{C}^N} \frac{1}{2} \sum_{\ell=1}^L \|\mathcal{F}_{\Omega} \mathcal{S}_{\ell} \boldsymbol{x} - \boldsymbol{y}_{\ell}\|_2^2 + \lambda g(\boldsymbol{x})$$

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MRI-NUFFT provides *efficient* implementation for the forward model operator:

- based on the NUFFT backend of your choice.
- Handles CPU/GPU transfers and array conversion (torch/numpy/cupy)
- autograd support $\frac{\partial \mathbf{A}x}{\partial x}$, $\frac{\partial \mathbf{A}^H y}{\partial y}$, $\frac{\partial \mathbf{A}_{\theta} x}{\partial \theta}$, ...

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```
from mrinufft import get_operator
nufft = get_operator("cufinufft", samples, shape, smaps=smaps,
density="pipe")
ksp = nufft.op(image)          #  $y = Ax$ 
adjoint = nufft.adj_op(ksp)    #  $x = A^H y$ 
pinv = nufft.pinv_solver(ksp)  #  $x = A^{\dagger} y$ , using CG
```

Extended Fourier Model

- Multi-coil, subspace representations, ...

Daval-Fr rot et al., MRM, 2022.; *Sutton et al.*, IEEE TMI, 2003.

Extended Fourier Model

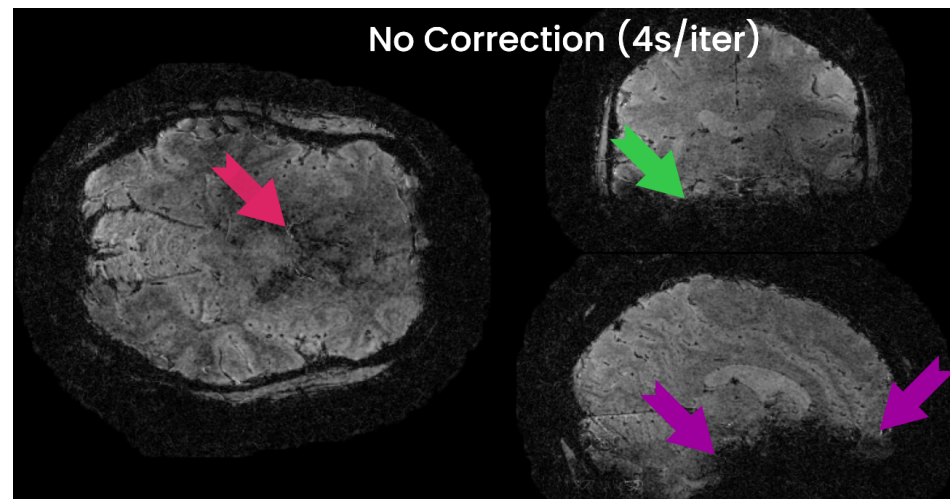
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Extended Fourier Model

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- Off-Resonance

$$\mathbf{y}_\ell(t) = \int_{FOV} \mathbf{x}(\mathbf{r}) \mathcal{S}_\ell(\mathbf{r}) e^{-\Delta\omega(\mathbf{r})t} e^{-2i\pi\mathbf{k}(t)\cdot\mathbf{r}} d\mathbf{r}$$



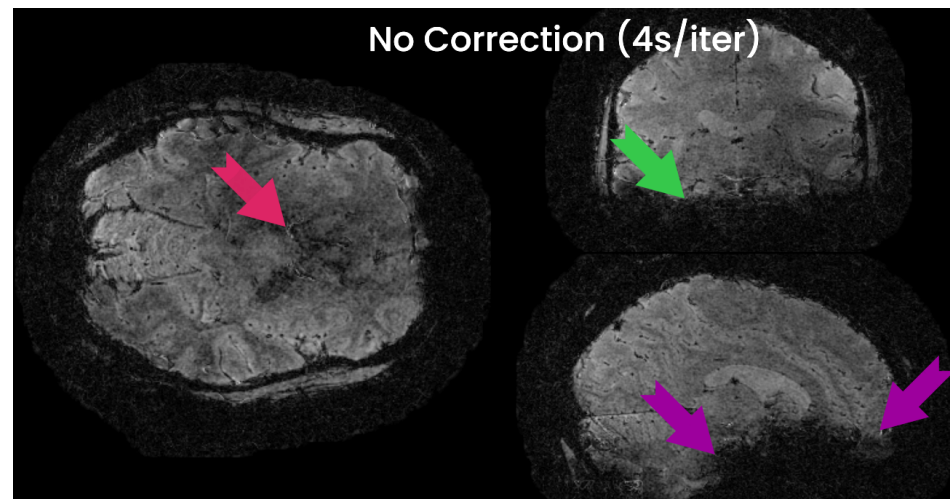
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Extended Fourier Model

- Multi-coil, subspace representations, ...
- Density Compensation (voronoi, pipe, ...)
- Off-Resonance correction via bilinearization (MTI, MFI)

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$$\mathbf{y}_\ell \approx \sum_{p=1}^P \mathbf{b}_p \sum_{\ell=1}^L \mathcal{F}_\Omega(\mathbf{c}_p \mathcal{S}_\ell \mathbf{x})$$



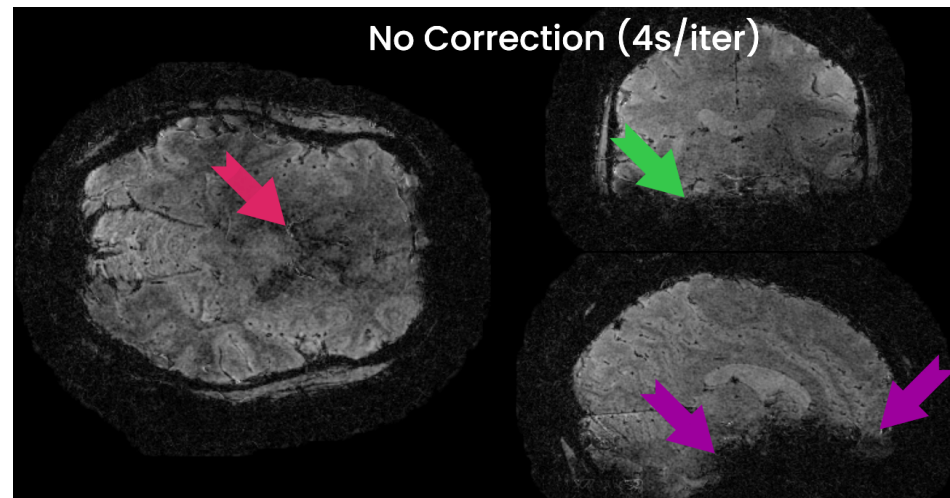
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$$\min_{\substack{\mathbf{B} \in \mathbb{C}^{M \times P} \\ \mathbf{C} \in \mathbb{C}^{P \times N}}} \|e^{-\Delta\omega(\mathbf{r})t} - \mathbf{BC}\|_2^2 \Rightarrow \mathbf{y}_\ell \approx \sum_{p=1}^P \mathbf{b}_p \sum_{\ell=1}^L \mathcal{F}_\Omega(\mathbf{c}_p \mathcal{S}_\ell \mathbf{x})$$



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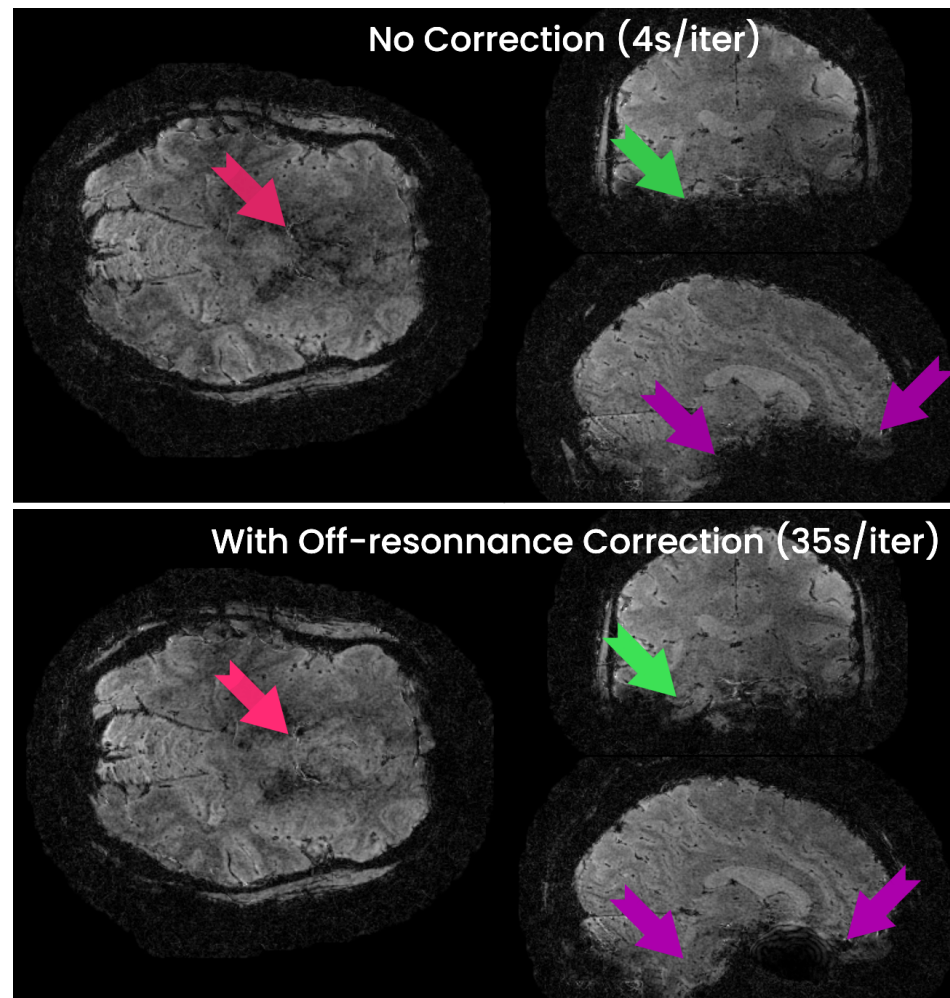
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```
nufft_orc = nufft.with_off_resonance_correction(  
    field_map=field_map,  
    readout_time=readout_time,  
    interpolators=20)  
adj_orc = nufft_orc.adj_op(ksp) #  $x = A_{\Delta\omega}^H y$   
pinv_orc = nufft_orc.pinv_solver(ksp) #  $x = A_{\Delta\omega}^\dagger y$ 
```

Daval-Fr rot et al., MRM, 2022.; Sutton et al., IEEE TMI, 2003.



Physics operators for Deep Learning



MRI-NUFFT Physics operator:

$$\mathbf{y} = f(\mathcal{S}, \Omega, \Delta\omega, \mathbf{x}) = A(\mathcal{S}, \Omega, \Delta\omega)\mathbf{x}$$

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■ In deep-learning application we rely on reverse-mode autodifferentiation

😓 VJP computations, complex derivatives and Wirtinger calculus

$$\left\langle \mathbf{v} \mid \frac{\partial A\mathbf{x}}{\partial \mathbf{x}} \right\rangle \quad \left\langle \mathbf{v} \mid \frac{\partial A^H \mathbf{y}}{\partial \mathbf{y}} \right\rangle \quad \left\langle \mathbf{v} \mid \frac{\partial A\mathbf{x}}{\partial \Omega} \right\rangle \quad \left\langle \mathbf{v} \mid \frac{\partial A\mathbf{x}}{\partial \mathcal{S}} \right\rangle \quad \dots$$

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 *Wang&Fessler, IEEE TCI, 2023.*

 Efficient implementation in MRI-NUFFT

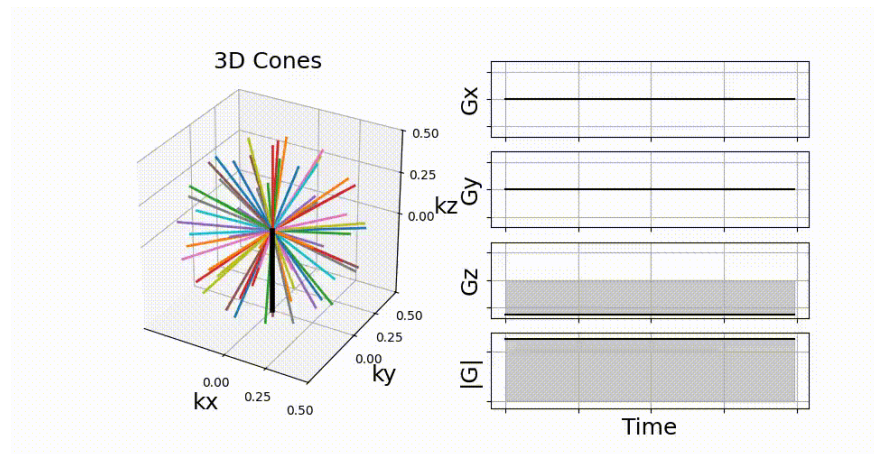
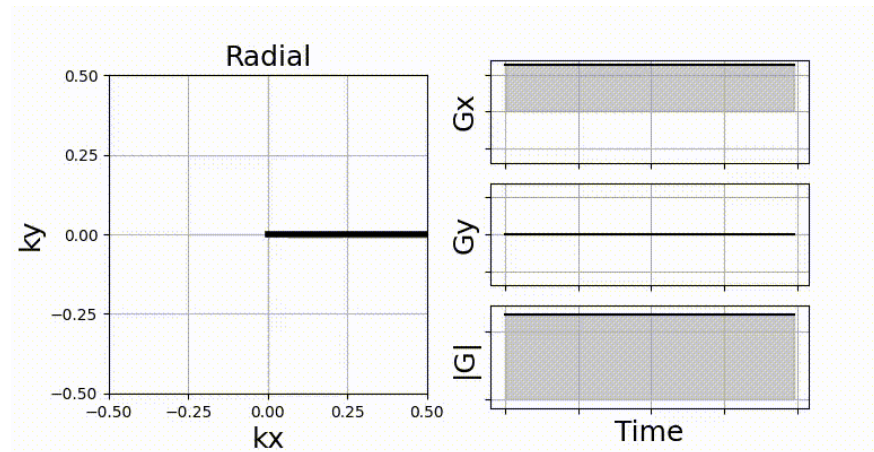
 WIP on $\frac{\partial A\mathbf{x}}{\partial \Delta\omega}$



3. Trajectories and Gradients

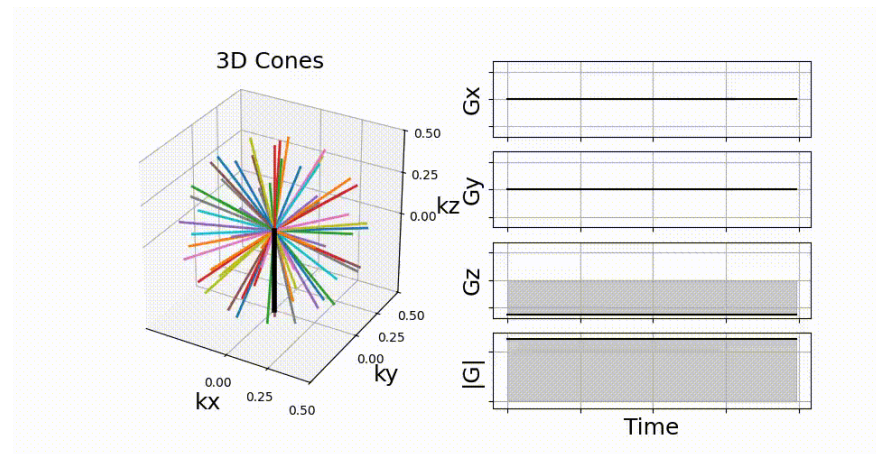
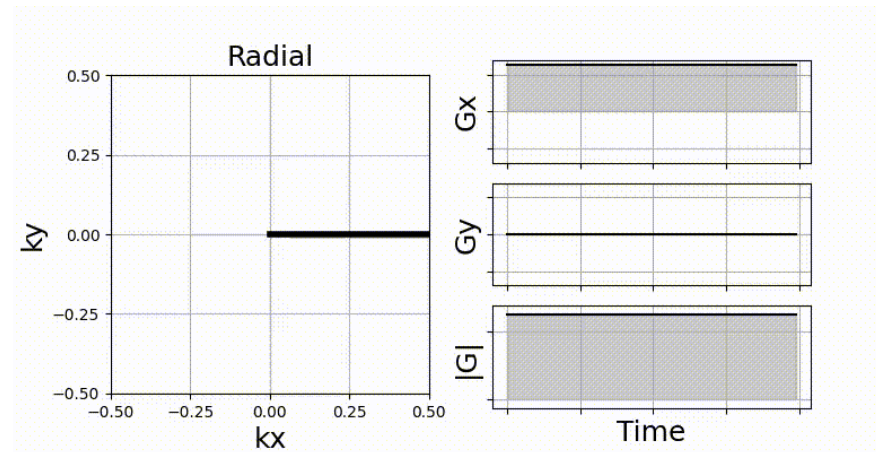
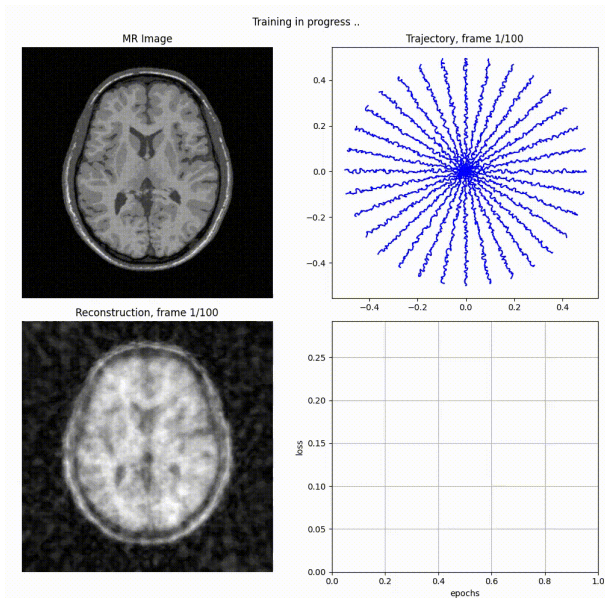
Trajectories & Gradients

- Large collection of non-Cartesian trajectories
- 2D and 3D, fully parameterized



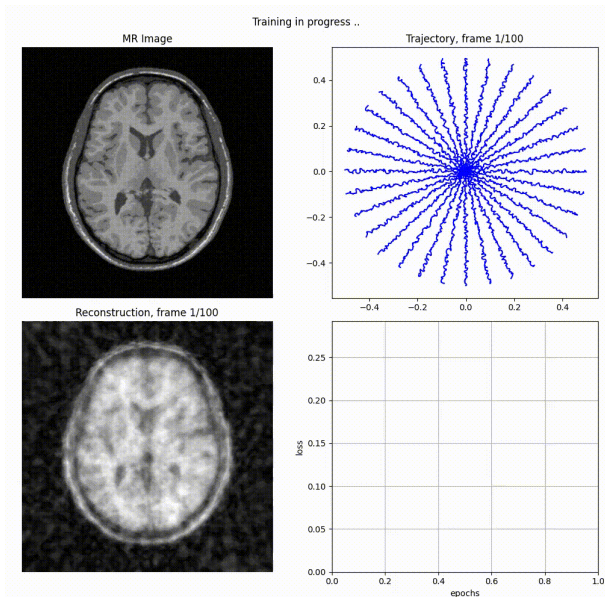
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- Large collection of non-Cartesian trajectories
 - 2D and 3D, fully parameterized
 - Hardware compliance enforcement.
 - You can even learn trajectories in a deep Learning setting with autodifferentiation !



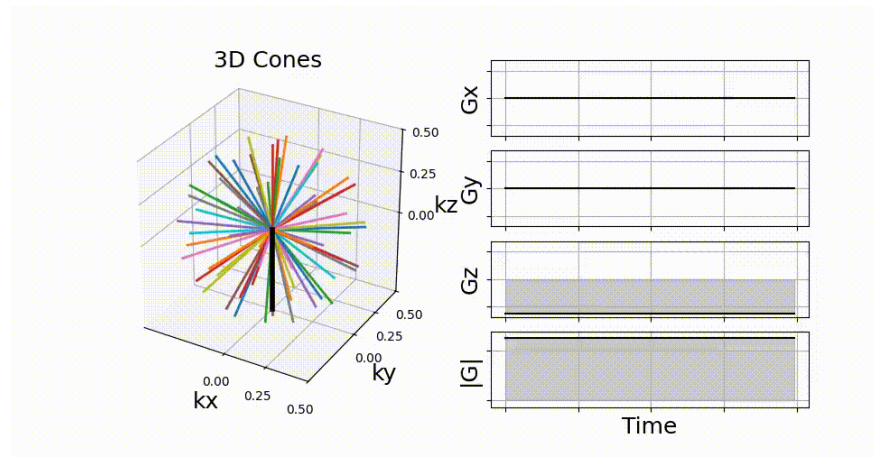
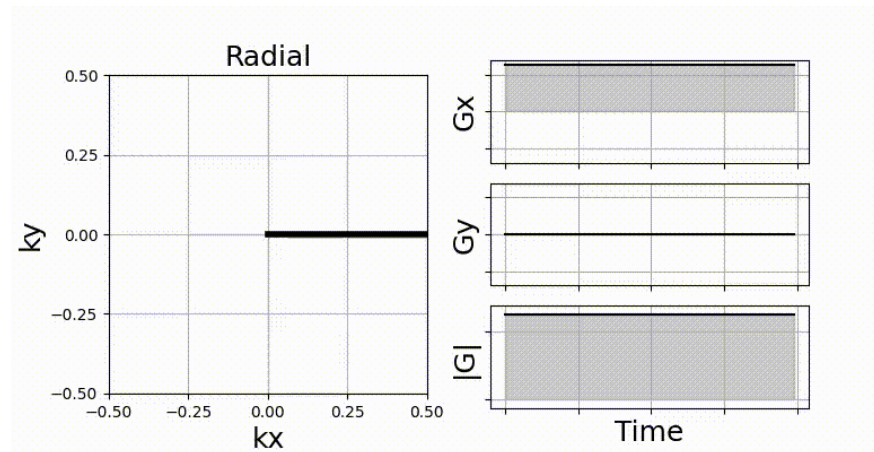
Trajectories & Gradients

- Large collection of non-Cartesian trajectories
 - 2D and 3D, fully parameterized
 - Hardware compliance enforcement.
 - You can even learn trajectories in a deep Learning setting with autodifferentiation !



Live Demo !

[Open in Colab](#)



Hardware compliant trajectories: Projection



Trajectories Constraints

Set of admissible trajectories

$$\mathcal{Q} = \left\{ \begin{array}{l} \forall i = \{1, \dots, N_c\}, \mathbf{k}_i \in \Omega^{N_s} \\ \|\mathbf{k}\|_{\infty} \leq \frac{1}{2}, \|\dot{\mathbf{k}}\|_{2,\infty} \leq G_{\max}, \|\ddot{\mathbf{k}}\|_{2,\infty} \leq S_{\max} \\ \mathbf{A}_i \mathbf{k}_i = \mathbf{b}_i \end{array} \right\}$$

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Given an existing trajectory $\mathbf{k} \in \Omega^{N_c \times N_s}$:

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Solved with a Primal Dual Algorithm *Chauffert et al.*,
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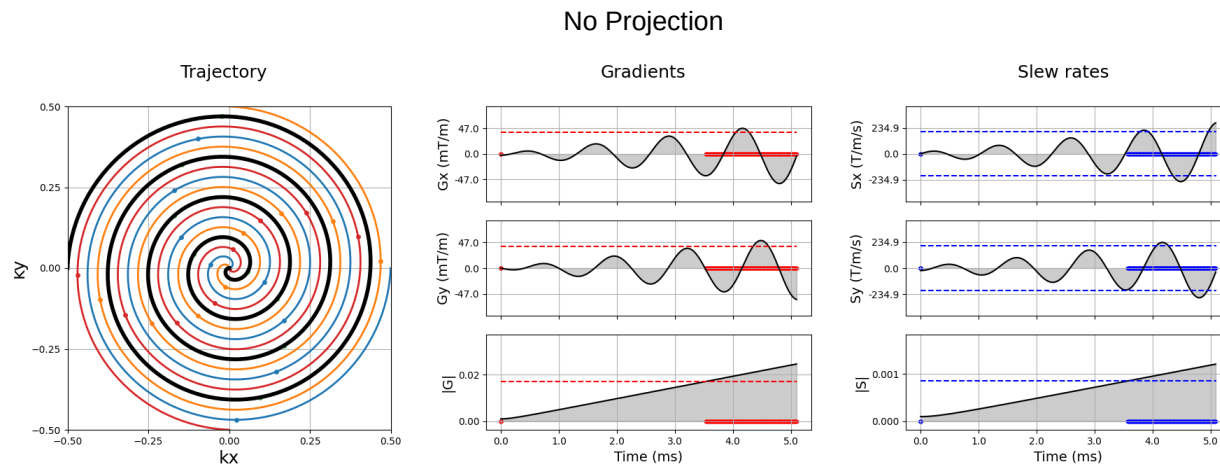
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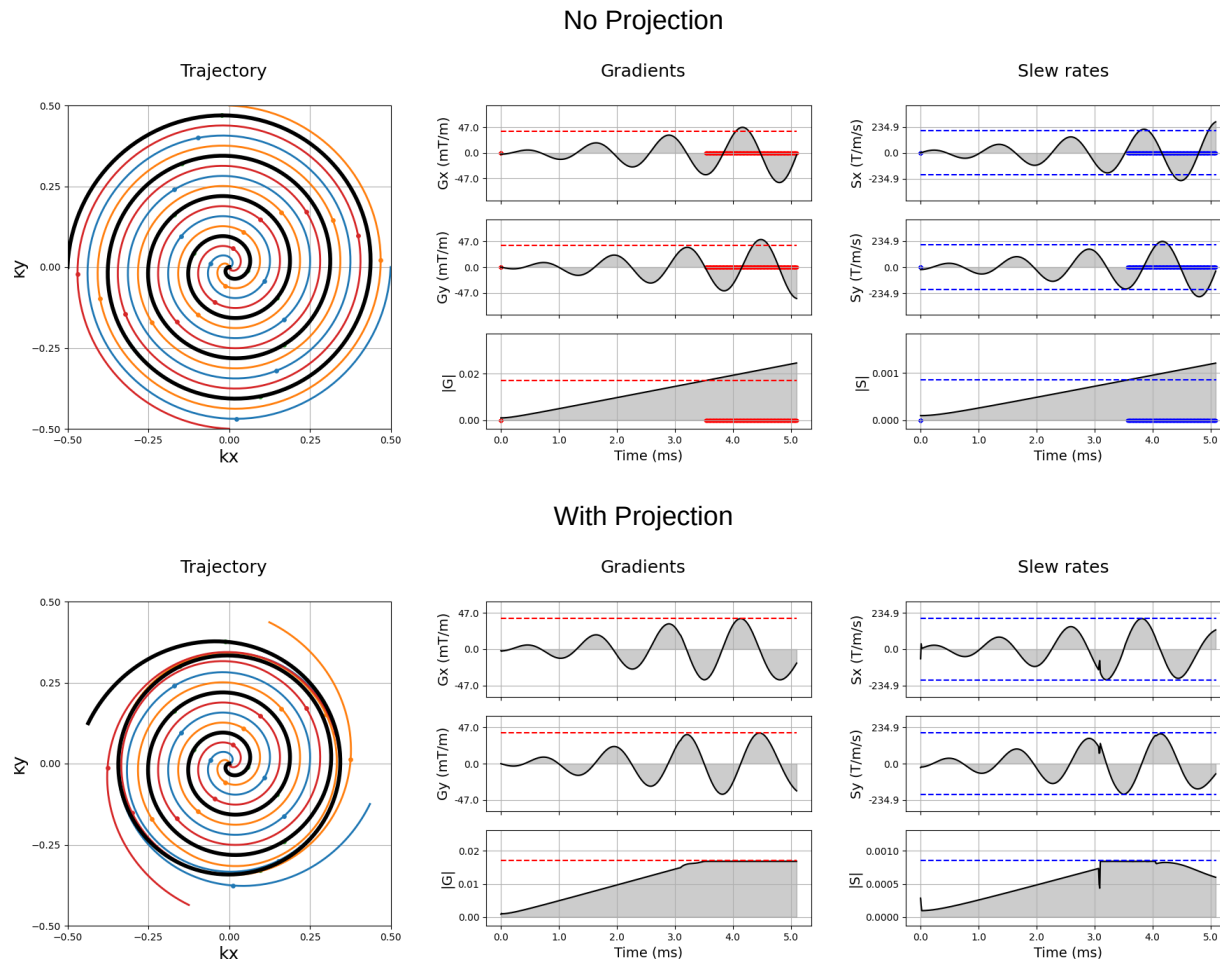
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Design Gradient Waveforms

Given $\|\dot{\mathbf{k}}\|_{\infty} \leq G_{\max}$, $\|\ddot{\mathbf{k}}\|_{\infty} \leq S_{\max}$, $\Delta \mathbf{k}$, $\mathbf{g}_{start}$, $\mathbf{g}_{end}$

1. What is the minimum of raster time points required?
2. Given this number of points, what is the path to take?
3. Make the trajectory as smooth as possible
 - minimize the slew rate OR
 - minimize curvature of gradients $\|\ddot{\mathbf{k}}\|$

Linear and Quadratic Programming



Linear Programming

Given a vector-size N , find $\mathbf{g} \in [-G_{\max}, G_{\max}]^N$ s.t.

$$\mathbf{A}_{\text{eq}} \mathbf{g} = \mathbf{b}_{\text{eq}} \quad \mathbf{A}_{\text{ub}} \mathbf{g} \leq \mathbf{b}_{\text{ub}}$$

$$\mathbf{A}_{\text{eq}} = \begin{bmatrix} 1 & 1 & \dots & 1 \\ 1 & 0 & \dots & 0 \\ 0 & 0 & \dots & 1 \end{bmatrix}, \quad \mathbf{b}_{\text{eq}} = \begin{bmatrix} \Delta k \\ \mathbf{g}_{\text{start}} \\ \mathbf{g}_{\text{end}} \end{bmatrix}$$

$$\mathbf{A}_{\text{ub}} = \begin{bmatrix} -1 & 1 & 0 & \dots \\ 0 & -1 & 1 & \dots \\ 1 & -1 & 0 & \dots \\ 0 & 1 & -1 & \dots \end{bmatrix}, \quad \mathbf{b}_{\text{ub}} = \begin{bmatrix} S_{\max} \Delta T \\ \vdots \\ S_{\max} \Delta T \end{bmatrix}$$

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Quadratic Programming

Smooth gradient $\rightarrow$ Minimize the curvature

$$\min_{\mathbf{g} \in \mathbb{R}^N} \sum_{i=0}^{N-1} (g_{i+1} - 2g_i + g_{i-1})^2 \quad \text{s.t. } g_n \in \mathcal{Q}$$

$$\min_{\mathbf{g} \in \mathbb{R}^N} \frac{1}{2} \mathbf{g}^T \mathbf{H} \mathbf{g} + \mathbf{q}^T \mathbf{g} + c \quad \text{s.t. } \mathbf{l} \leq \mathbf{A} \mathbf{g} \leq \mathbf{u}$$

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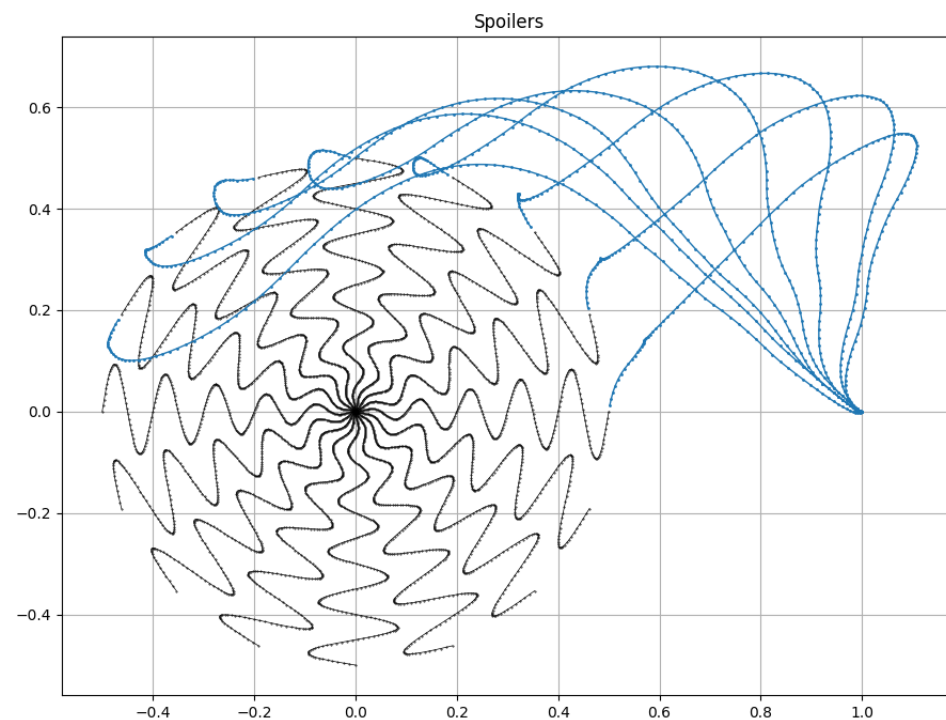
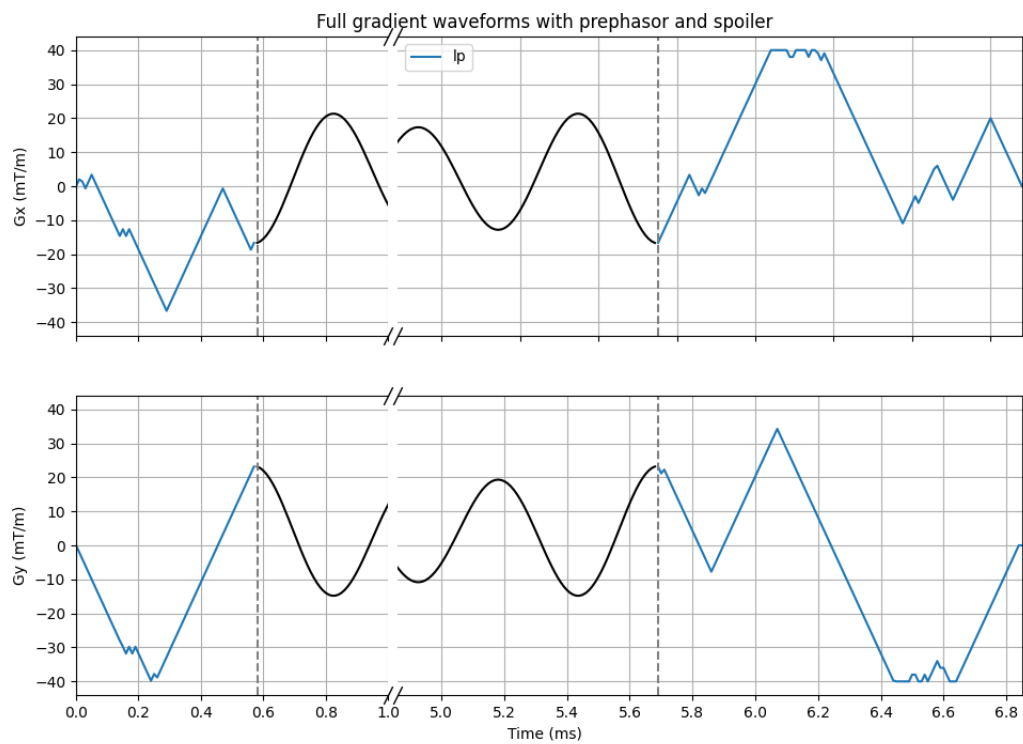
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- There exist an N_0 s.t. $\forall N \geq N_0, \Delta k \in \left\{ \sum_n^N g_n \mid g_n \in \mathcal{Q} \right\}$
- Finding N_0 is done with binary search
 - Is it feasible $\Leftrightarrow$ Solve it
 - Engineer trick: quantize the constraints for multi-shot setting ($N_{\text{shots}} \times 3 \leadsto 100$ -ish cases)
 - Same mini-max N for all shots (same TR !)



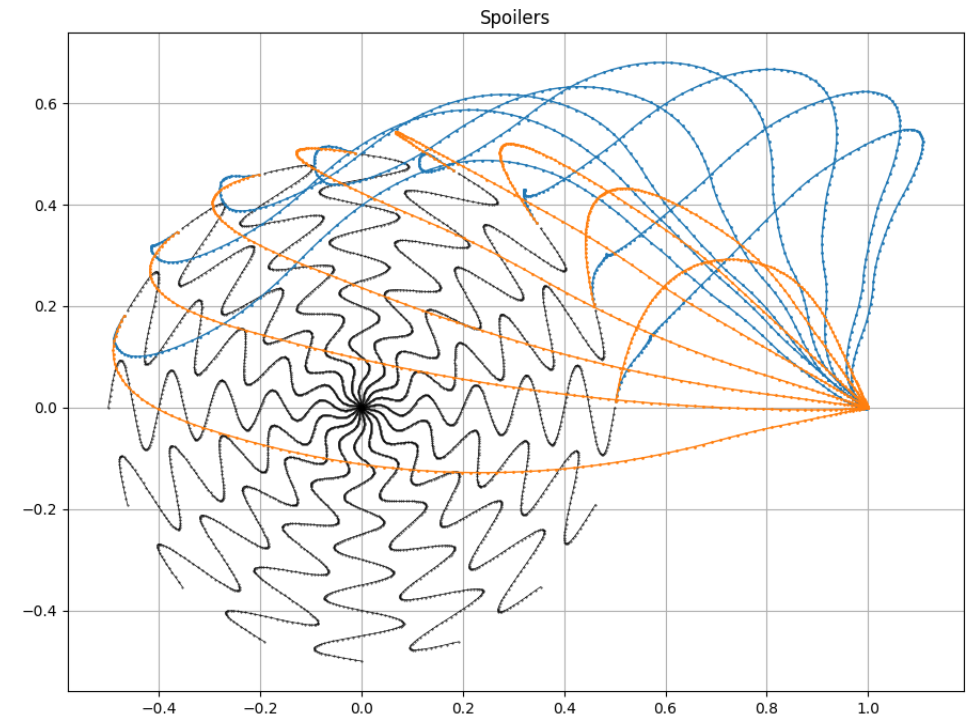
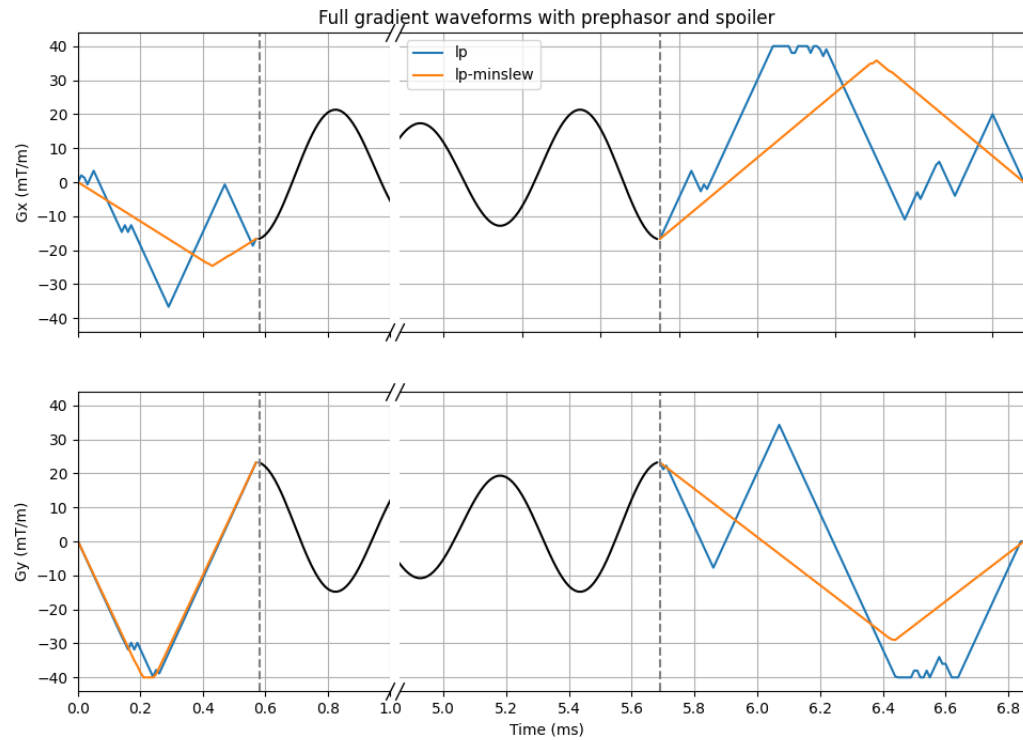
Linear Programming



Connecting the dots

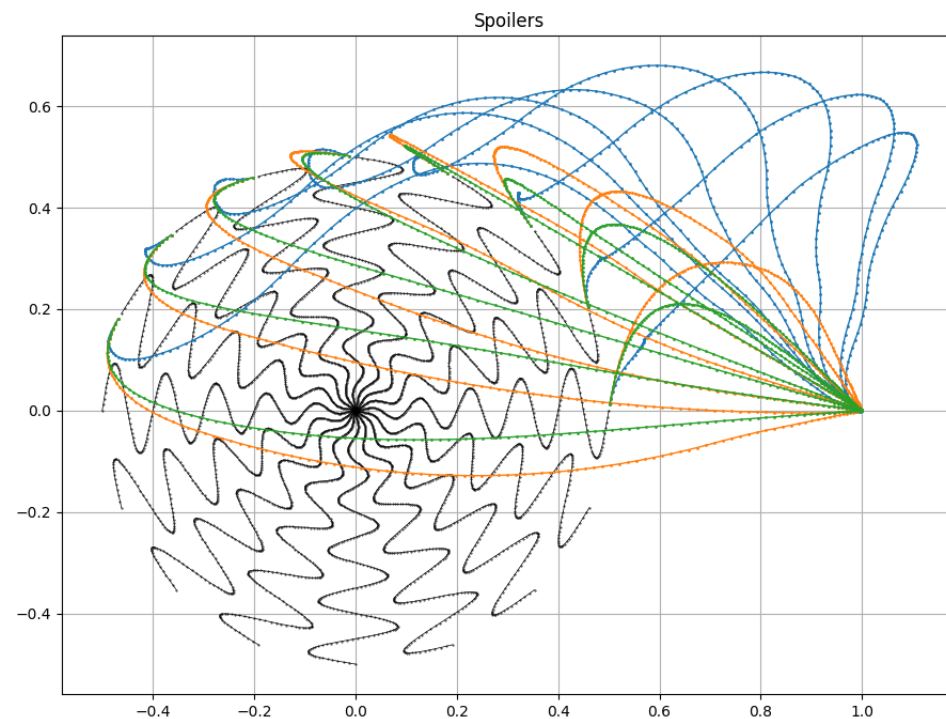
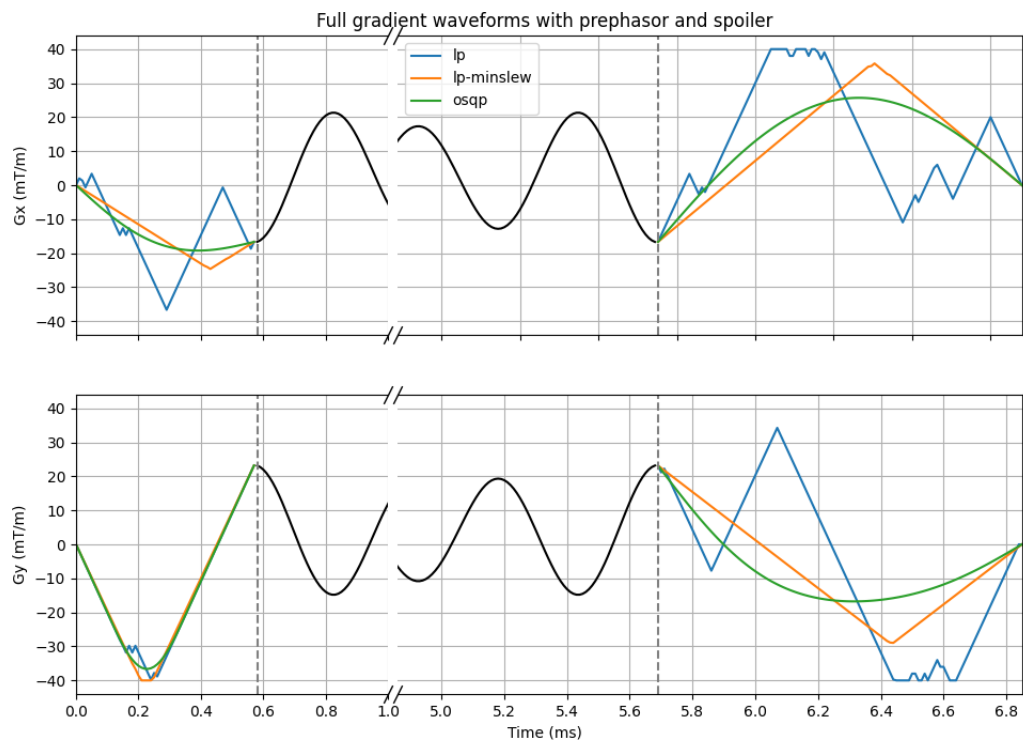


Linear Programming + Mini-Max Slew Rate (binary searched again)





Quadratic Programming





4. ■ The toolbox part

Integration with other libraries



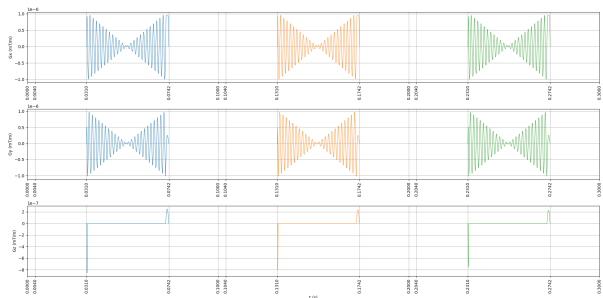
- ≥ 20 Projects depends on MRI-NUFFT¹
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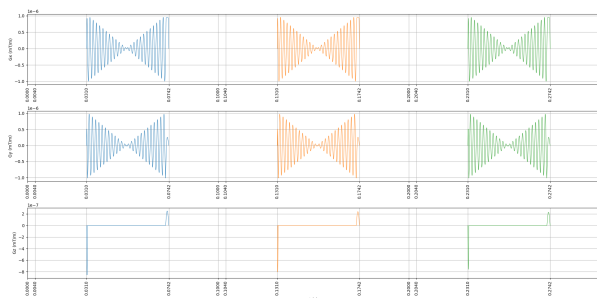


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Example for integration with deepinv

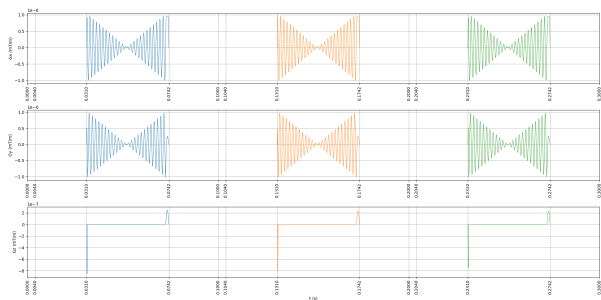
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fourier_op = get_operator("cufinufft", samples_loc, shape=shape)
y = fourier_op.op(ground_truth) + noise #  $y = Ax + \epsilon$ 
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# DeepInverse setup
physics = fourier_op.make_deepinv_phy()
wavelet = WaveletPrior(wv="sym8", is_complex=True, p=1) #  $\|\Psi \cdot\|_1$ 
wavelet_fista = optim_builder(
    iteration="FISTA",
    prior=wavelet, # swap with ANY prior !
    data_fidelity=L2(),
    params_algo={"lambda": 0.1}
)

# Reconstruction
x_pinv = physics.A_dagger(y) #  $\arg \min_x \|Ax - y\|_2^2$ 
x_wavelet = wavelet_fista(y, physics) #  $\arg \min_x \|Ax - y\|_2^2 + \lambda \|\Psi x\|_1$ 
```

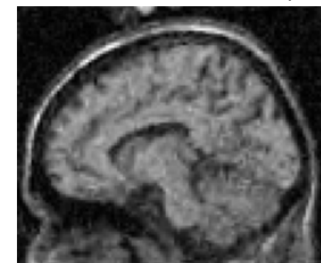
Ground truth



Adjoint reconstruction



Reconstruction with wavelet prior



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Conclusion

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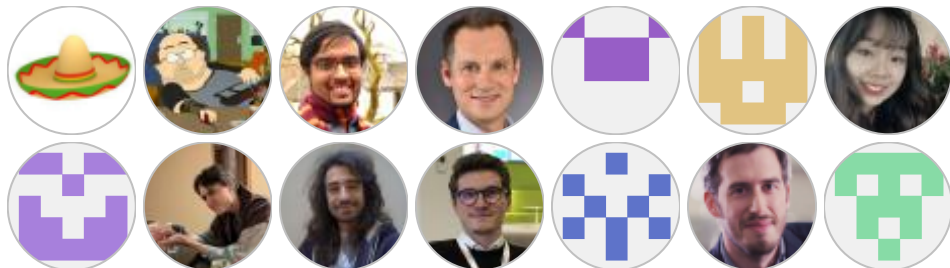
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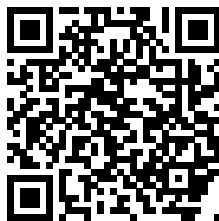
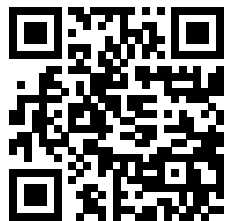


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Comby et al., (2025). *MRI-NUFFT: Doing non-Cartesian MRI has never been easier*. Journal of Open Source Software, 10(108), 7743, <https://doi.org/10.21105/joss.07743>

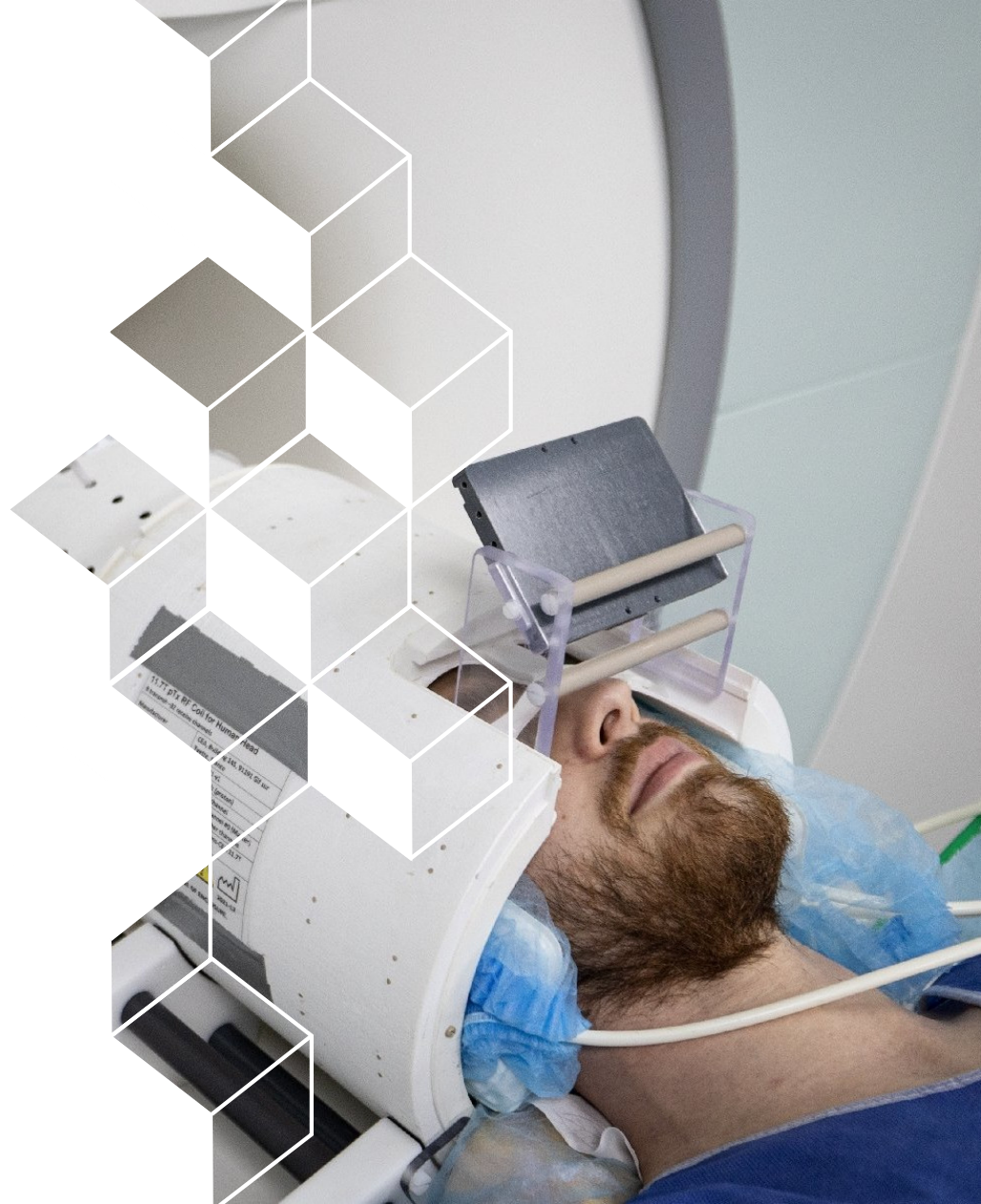
Check out Our awesome **open-source** software:



Thank you for your attention

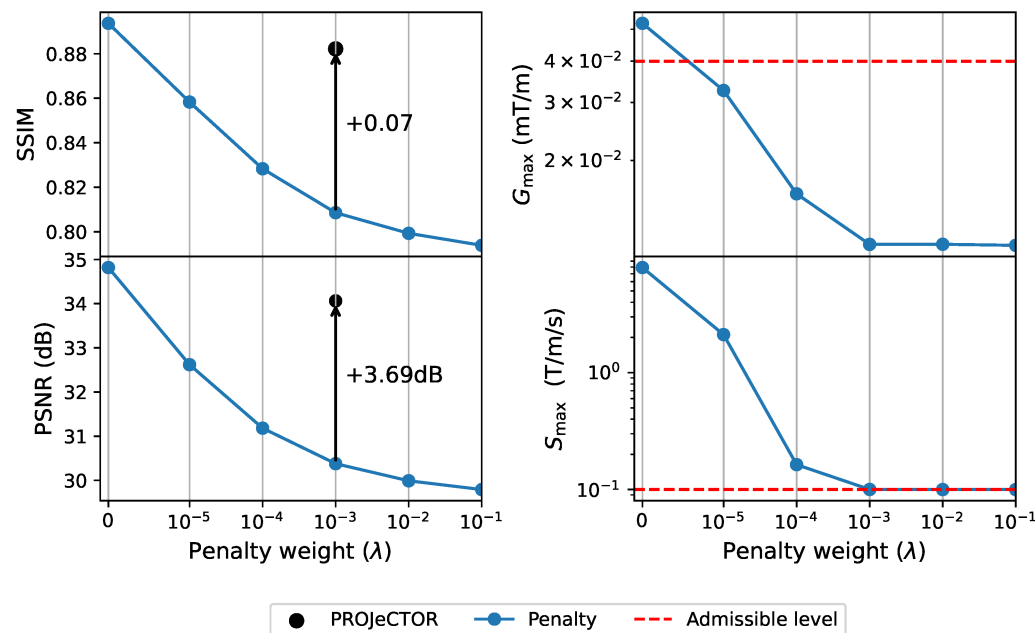
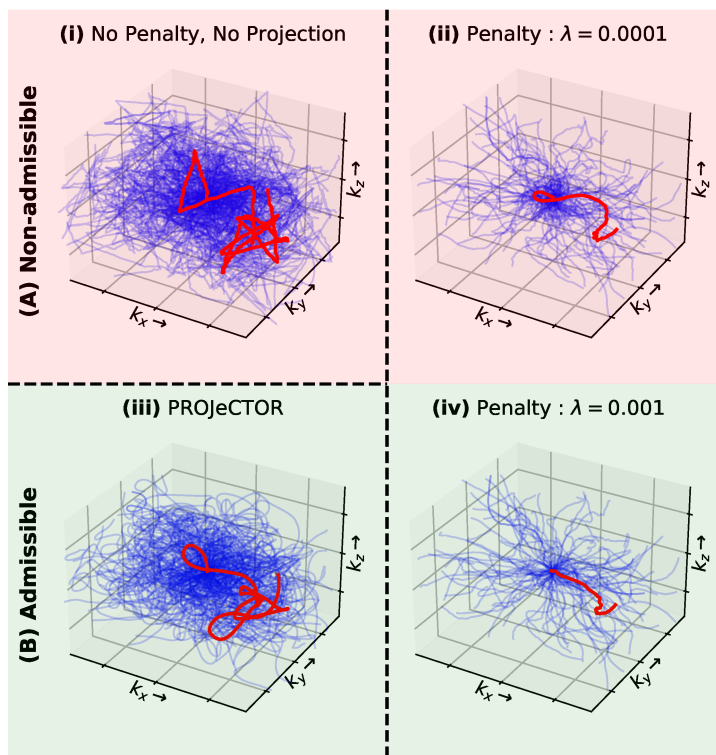
pierre-antoine.comby@cea.fr

Neurospin, CEA, Paris-Saclay University

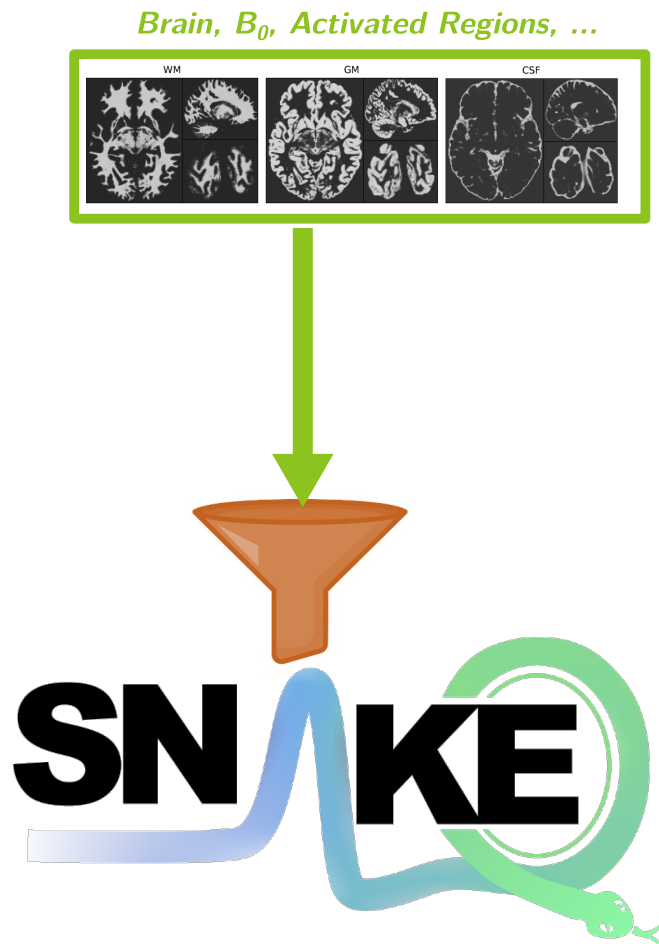


Projection vs penalty for trajectory design

- Context: Learning the trajectory $\partial \frac{A}{\partial} \Omega$ (+Joint reconstruction network)
- *Radhakrishna&Ciuciu, Bioeng., 2023.*



SNAKE fMRI k-space Simulator



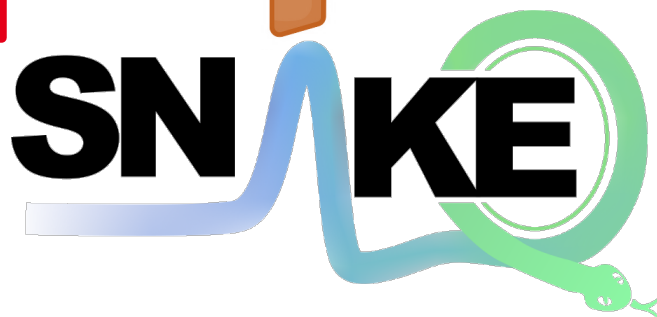
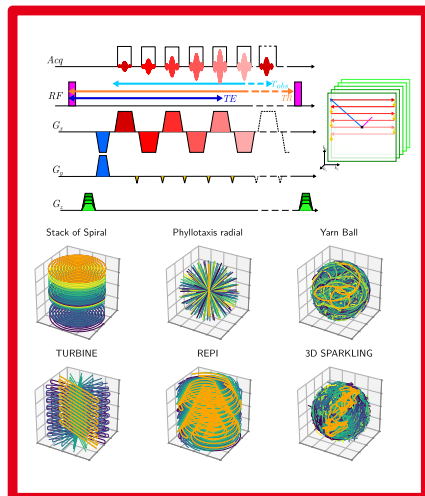
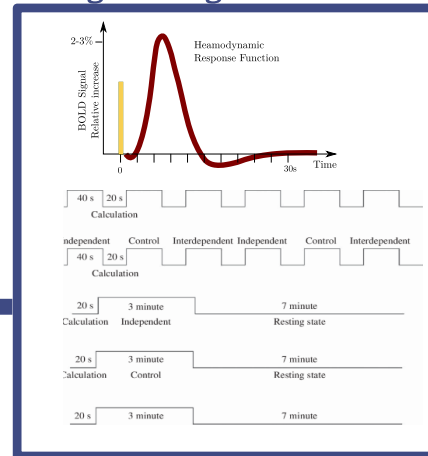
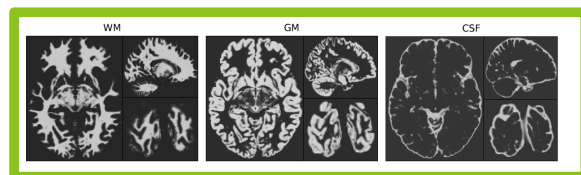


SNAKE fMRI k-space Simulator

Brain, B_0 , Activated Regions, ...

Paradigm Design & HRF model

Acquisition Setting

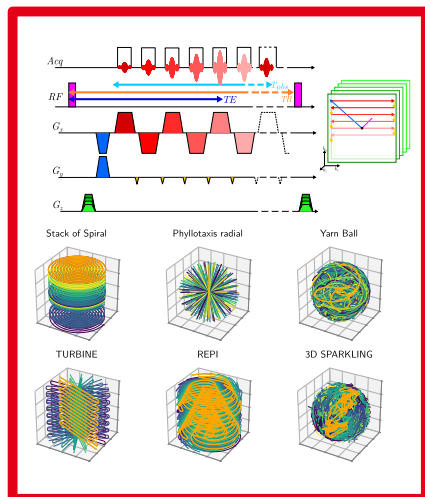
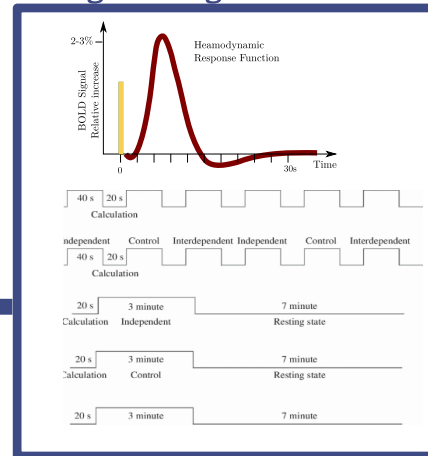
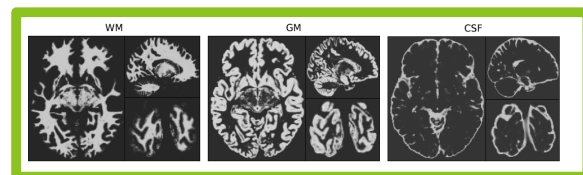


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SN  **KE**

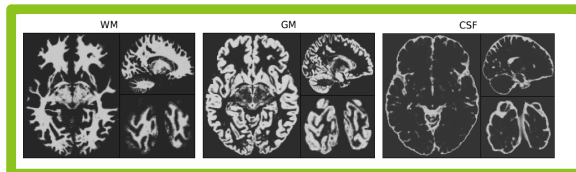
RECONSTRUCTION

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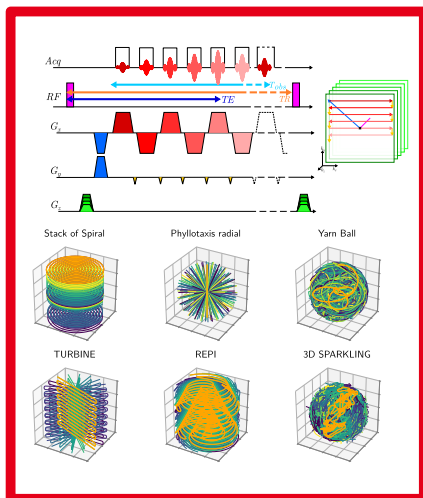
Learn more

Comby et al., ImagNeuro, 2025.

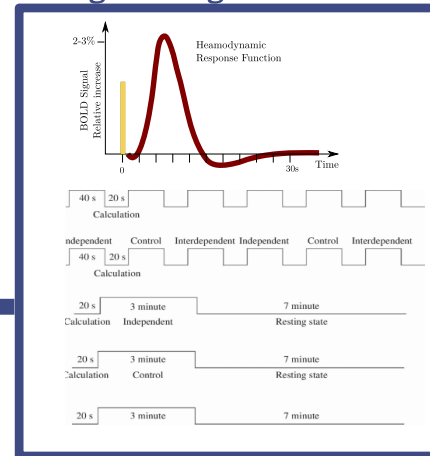
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SNKE

RECONSTRUCTION

STATISTICAL
ANALYSIS
VALIDATION